

Nanophotonic silicon-based biosensors and biochips

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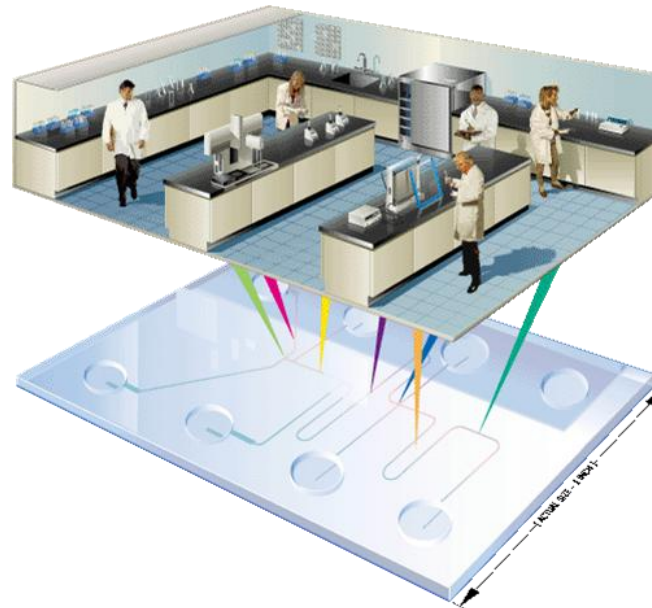
Naples, Italy



One of the new frontiers of the
“information age”, based on silicon
technology, is the realization of
photonics devices integrated on chip
capable of manipulating light at the
nanoscale

...and also the realization of new chips capable of performing complex functions:

- to sense and interact with the environment
- manipulate fluids
- to be remotely interrogated and powered



tries^{3,4}. For example, of the world's population of 6.1 billion people, 3 billion lack basic sanitation, 2 billion do not have access to electricity and more than 1 billion lack basic healthcare services and clean drinking water^{5,6}. For every public health triumph such as the



- ***1 billion, or half of the world's children, live in poverty***
- ***more than half the deaths in the poorest countries are the result of infection diseases (compared to 5% in the richest ones)***

[Source: P. Yager, et al., Nature, Vol. 442, 27 July 2006)]

Microfluidic diagnostic technologies for global public health

Paul Yager¹, Thayne Edwards¹, Elain Fu¹, Kristen Helton¹, Kjell Nelson¹, Milton R. Tam² & Bernhard H. Weigl³

The developing world does not have access to many of the best medical diagnostic technologies; they were designed for air-conditioned laboratories, refrigerated storage of chemicals, a constant supply of calibrators and reagents, stable electrical power, highly trained personnel and rapid transportation of samples. Microfluidic systems allow miniaturization and integration of complex functions, which could move sophisticated diagnostic tools out of the developed-world laboratory. These systems must be inexpensive, but also accurate, reliable, rugged and well suited to the medical and social contexts of the developing world.

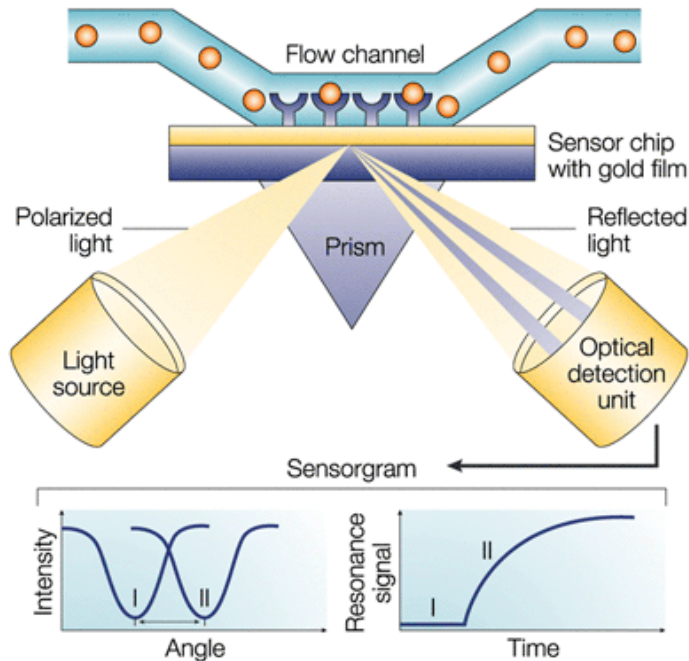
Challenges in biomedicine

- New technologies for small, cheap, reliable point-of-care testing (label free nanosensor arrays and lab-on-chips) for instant diagnostic, in any place at any time
- Very high sensitive biosensors, with extremely low detection limits for early stage disease detection
- Ultra-high resolution microscopy (below the diffraction limit) for real time sub-cellular imaging
- Micro and nano-systems for smart drug delivery (*i.e.*, in cancer therapy)

Negative photonic crystals
to trap light at the nanoscale
and excite optical resonances
...useful in biosensing

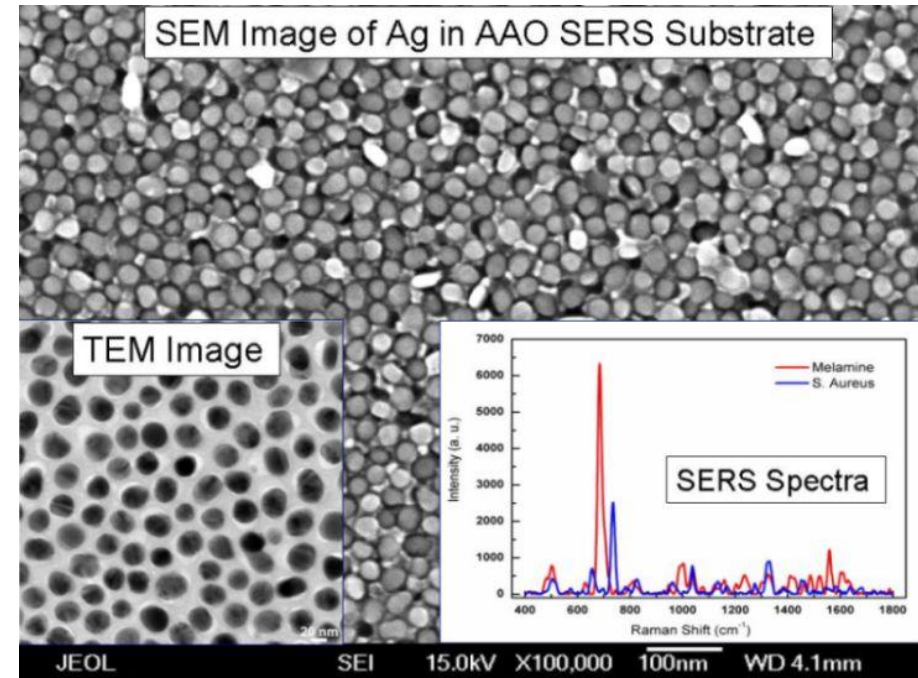
Well known applications of plasmonic resonances in biosensing

Surface plasmon resonance (SPR) sensors



Nature Reviews Drug Discovery 1, 515-528 (2002)

Surface enhanced raman spectroscopy based on localized-SPR effect

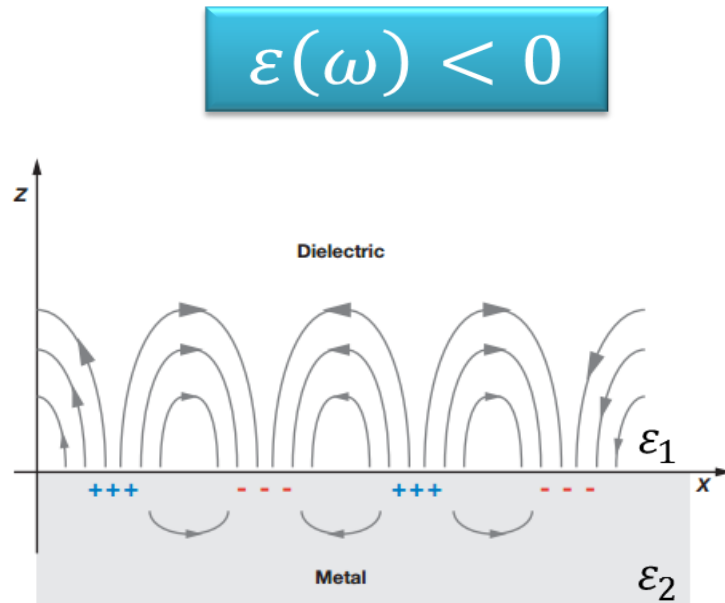


Advanced Materials 18, 491 (2006)

- label free technique
- real-time detection
- high enhancement factors

Analogy between...

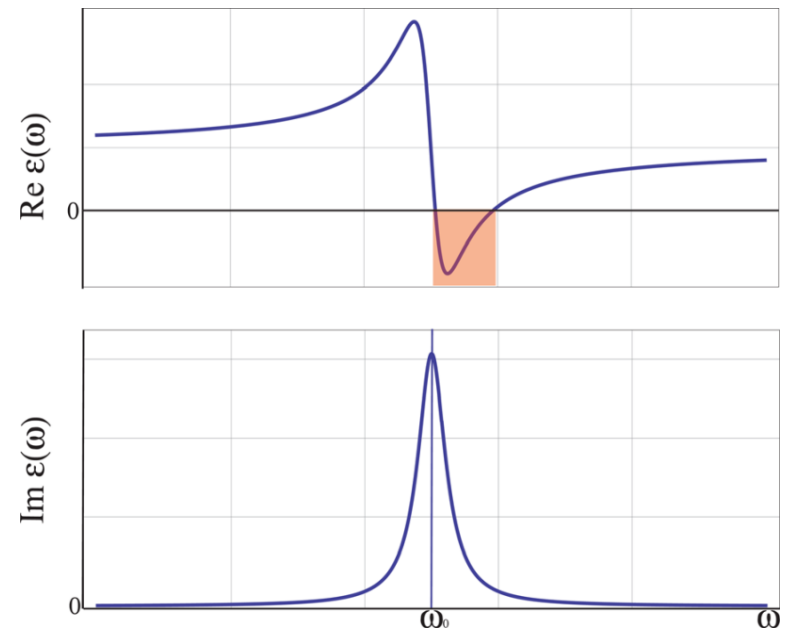
...metal plasmonic structures



Metals: Drude model

$$\epsilon = \epsilon_0 - \omega_p^2 / (\omega^2 - i\gamma\omega)$$

... non-metal negative photonic crystals



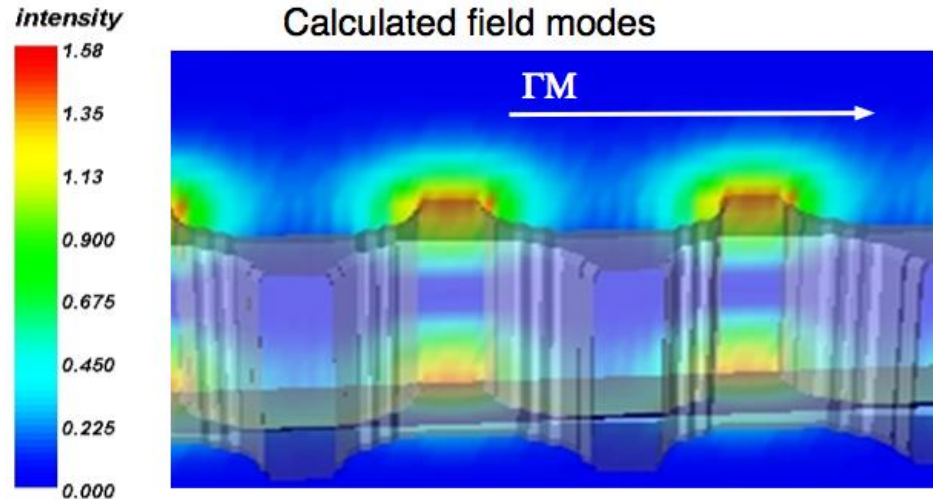
Non-metals: Lorentz model

$$\epsilon = \epsilon_\infty + f \omega_0^2 / (\omega_0^2 - \omega^2 + j\gamma\omega)$$

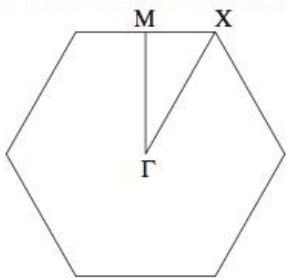
Our idea: to *exite* *plasmon-like* resonances at the interface with *negative dielectric* photonic crystals, so avoiding:

- optical absorption in metals
- resonance peak broadening
- local unwanted heating

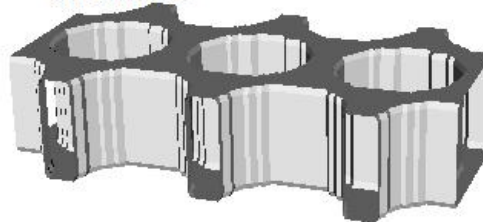
Finite Difference Time Domain simulations in a 2D negative PhC



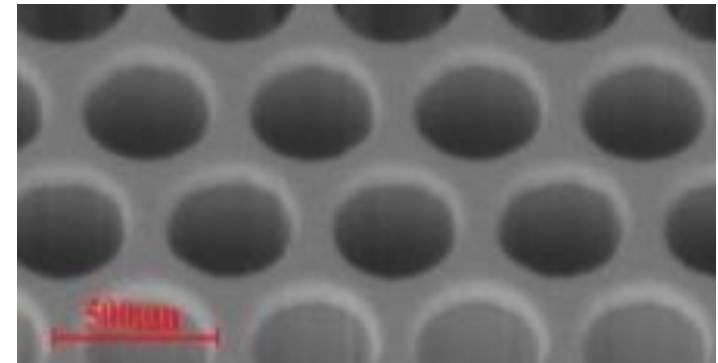
First Brillouin zone



Structure



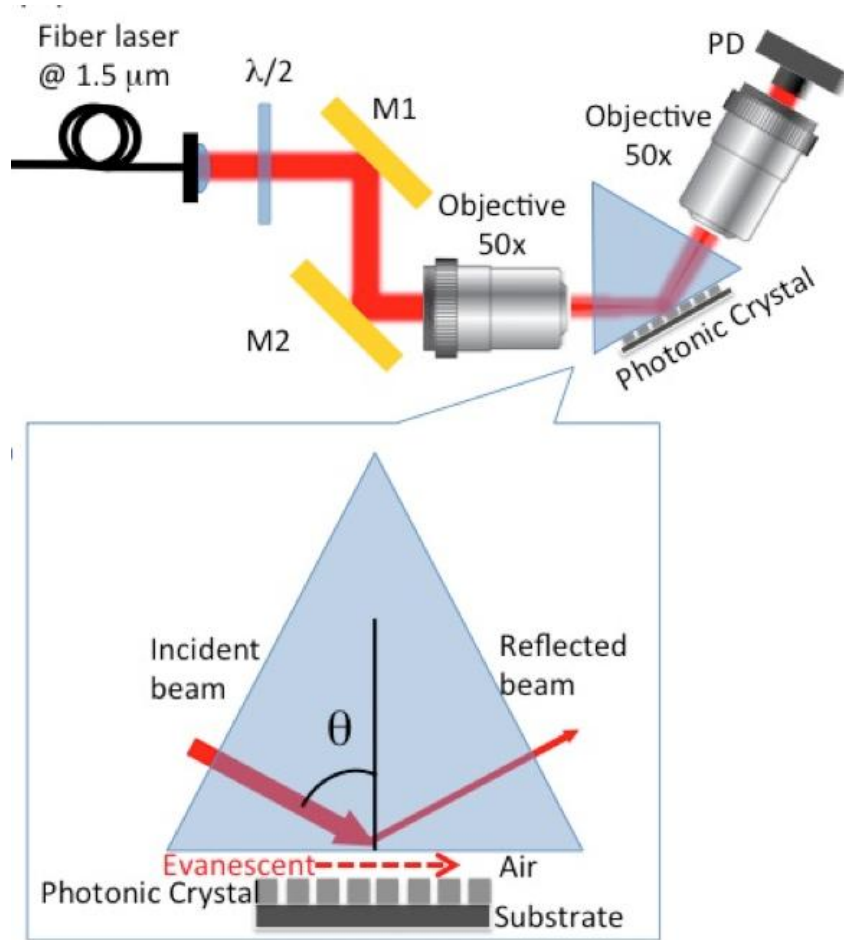
Device realization



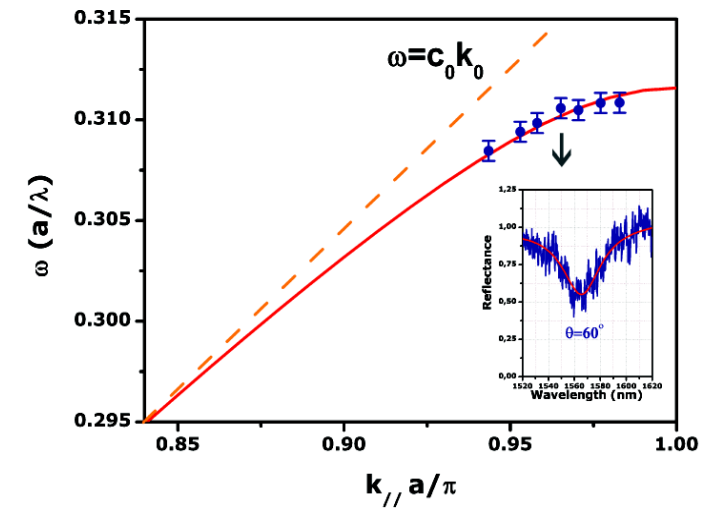
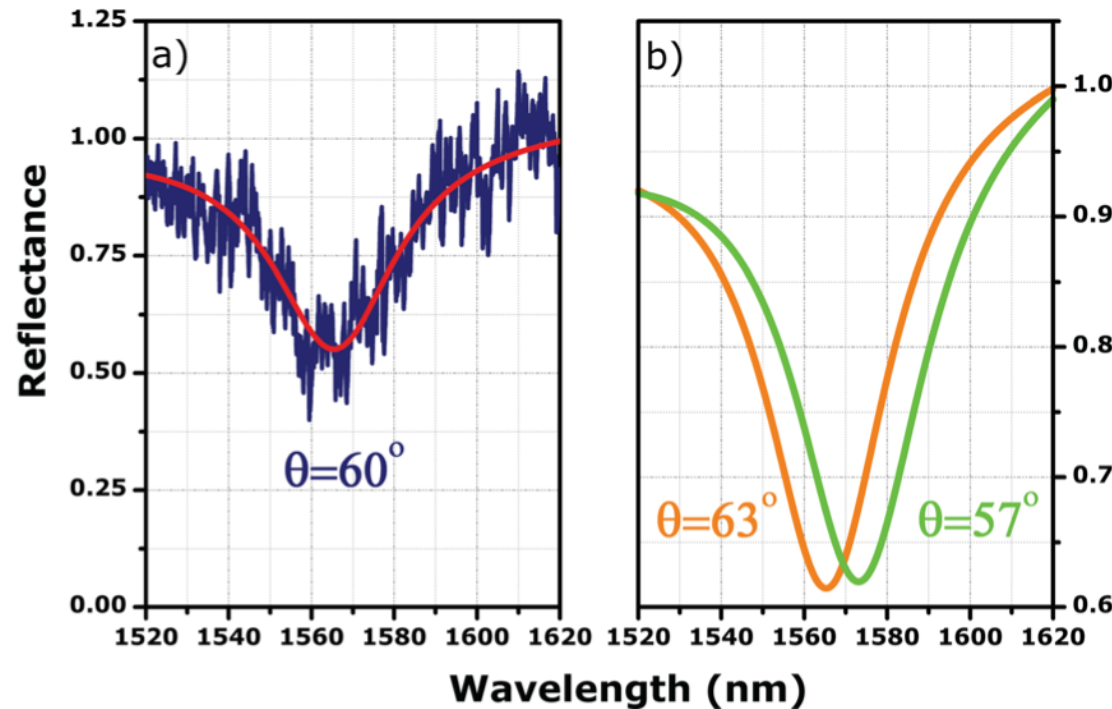
2D PhC silicon slab on a SOI wafer

- Lattice constant a : 472 nm
- Hole radius r : $0.385a$
- Thickness: 700 nm
- Effective negative refractive index around normalized frequency $a/\lambda=0.31$

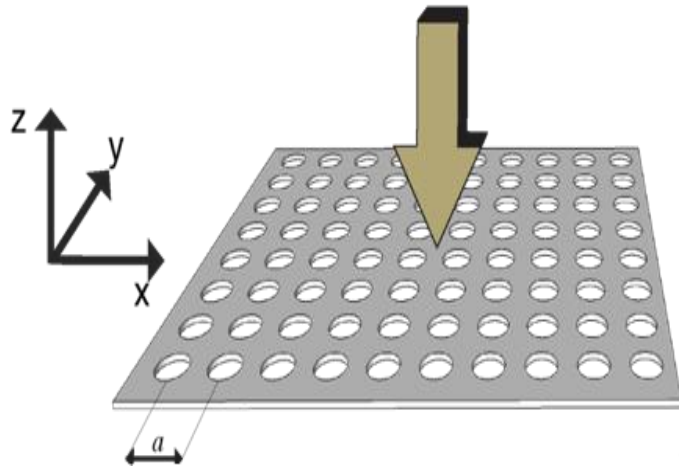
Plasmon-like surface states: experimental characterization



Experimental evidence of plasmon-like resonances

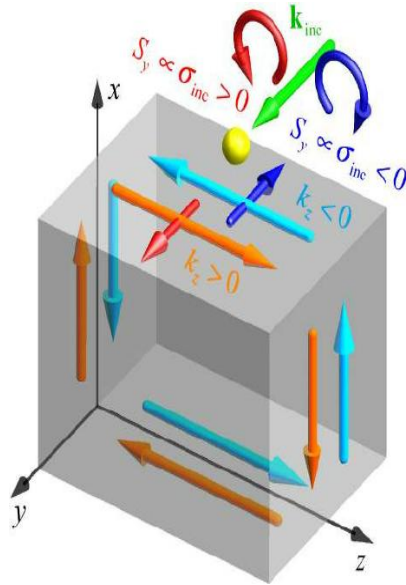


Sharp distributed resonances by exciting Bound States in Continuum (BICs) of radiation modes



- ❖ Normal-to-the-surface configuration
- ❖ Distributed resonances
- ❖ Easy and reliable coupling of light to PhC
- ❖ High enhancement of the E-field at the PhC interface
- ❖ High-Q resonators
- ❖ Good tolerance to fabrication imperfections

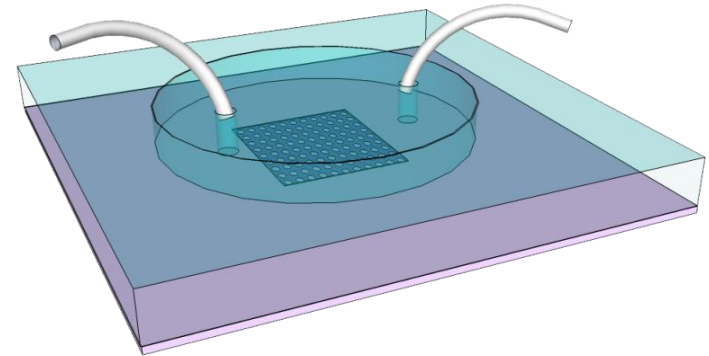
- ❖ Distributed resonances with predicted infinite lifetimes
- ❖ Fabrication imperfections and the finite extent of the structure partially break the crystal symmetry allowing the coupling of these resonances, and the excitation of evanescent surface waves



Qubit manipulation by optical Quantum Spin-Hall Effect

Design and realization of new sensors:

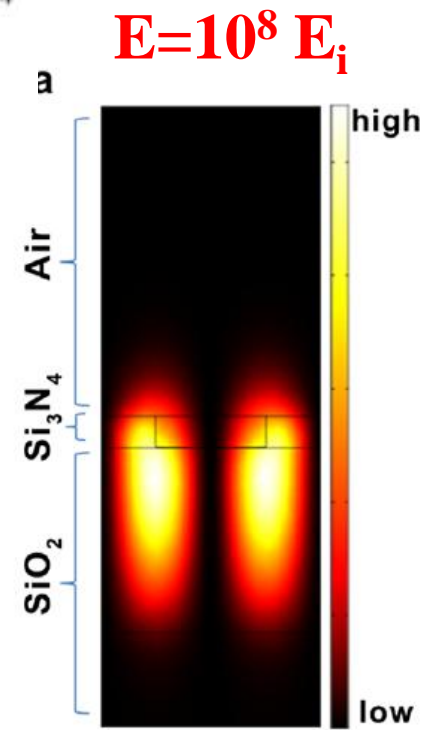
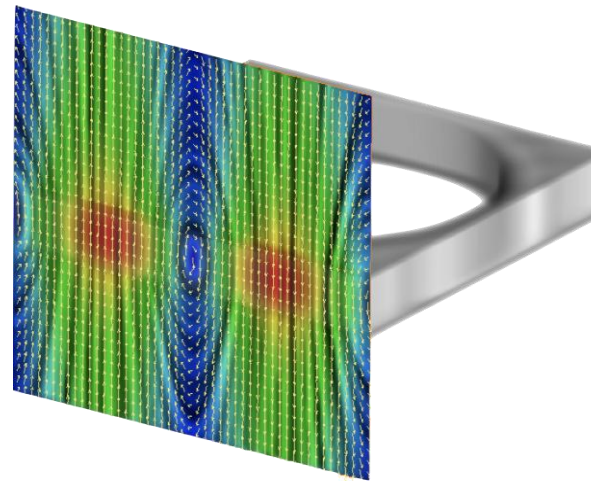
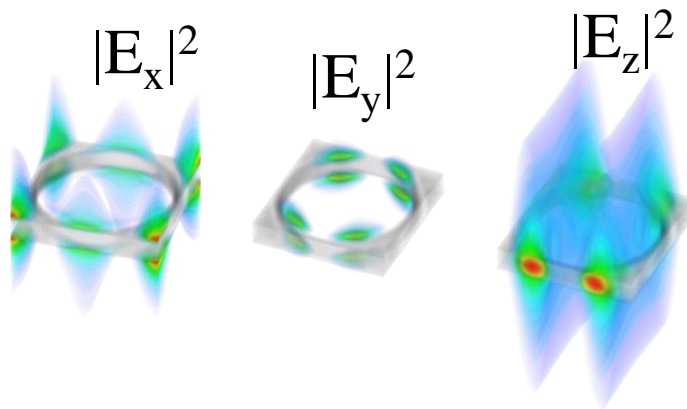
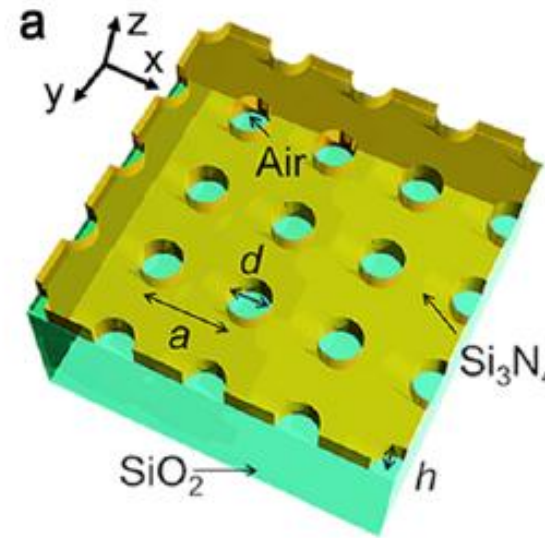
nanostructured surfaces where light is
confined and enhanced, enabling very
high sensitivities



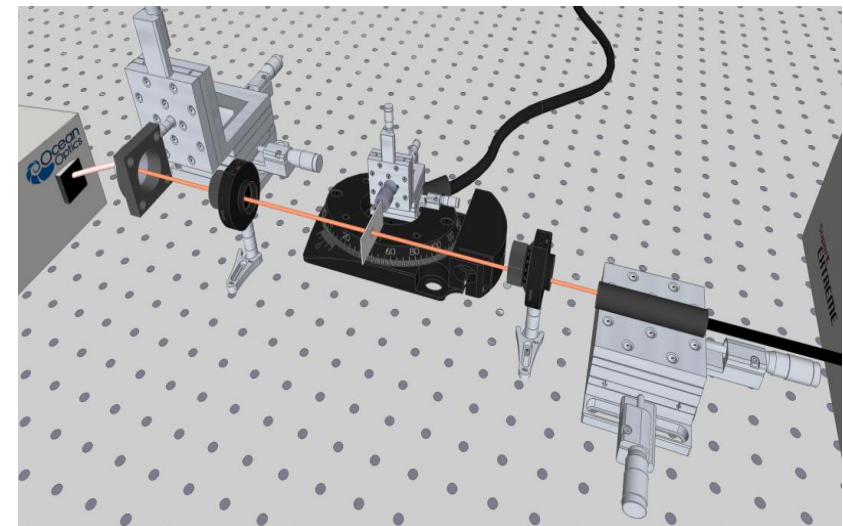
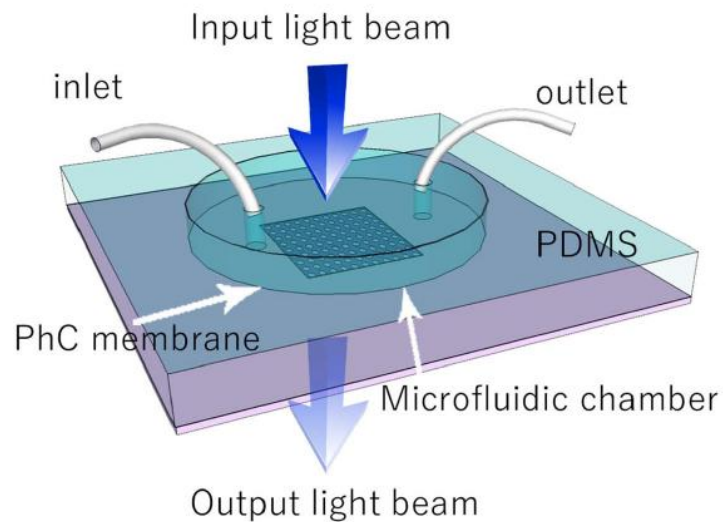
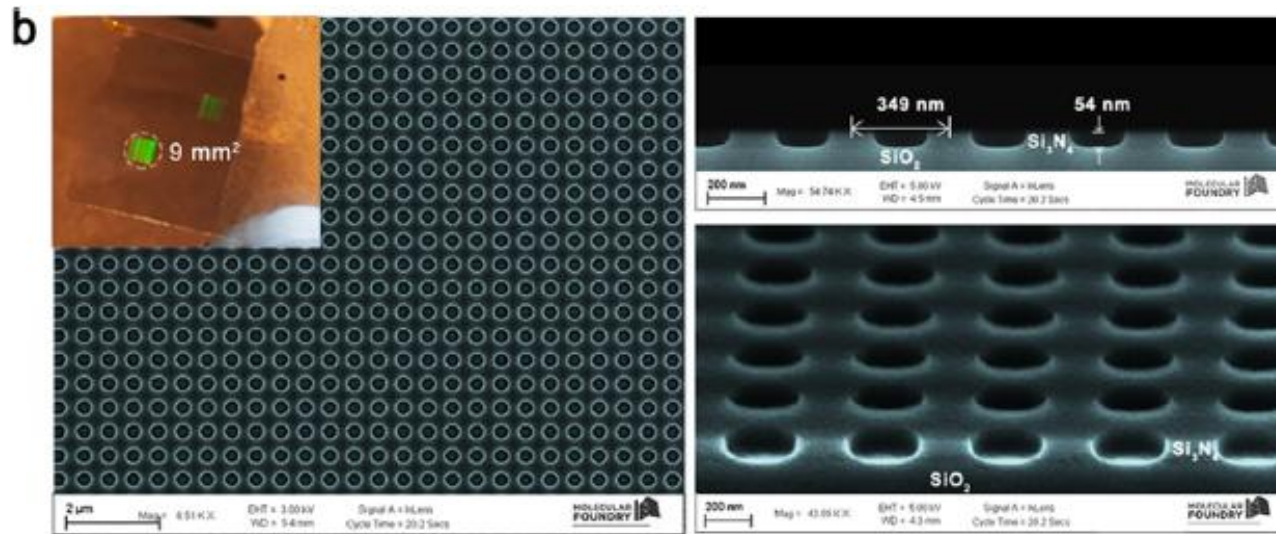
PhC sensing surface design

- 2D-PhC in Si_3N_4 ($n \sim 2$; $h \sim 60$ nm)
on a SiO_2 substrate
- square lattice of cylindrical holes
 $a \sim 500$ nm; $d \sim 130$ nm

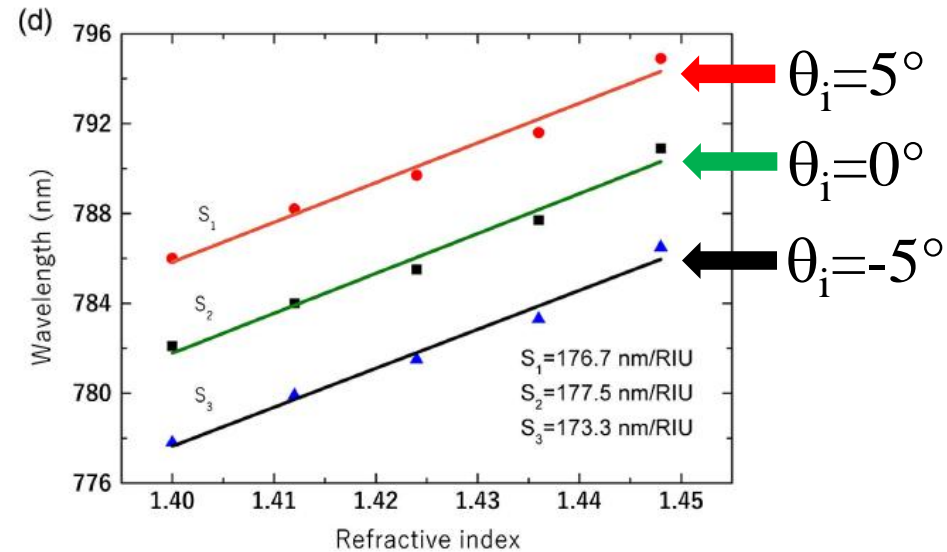
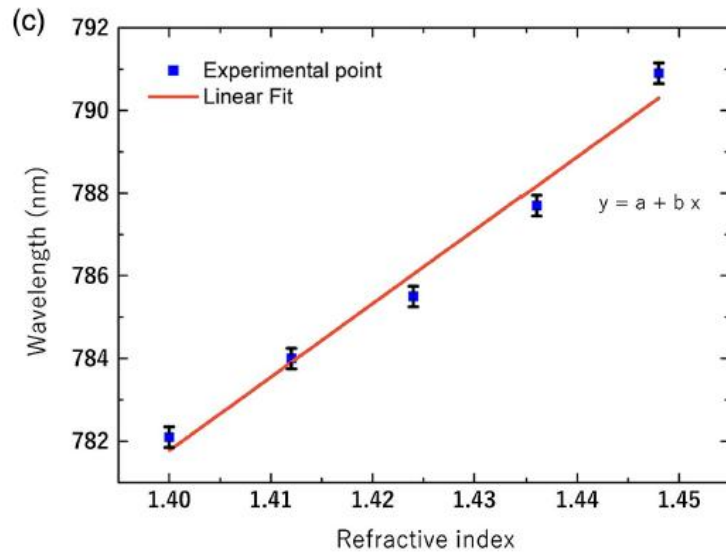
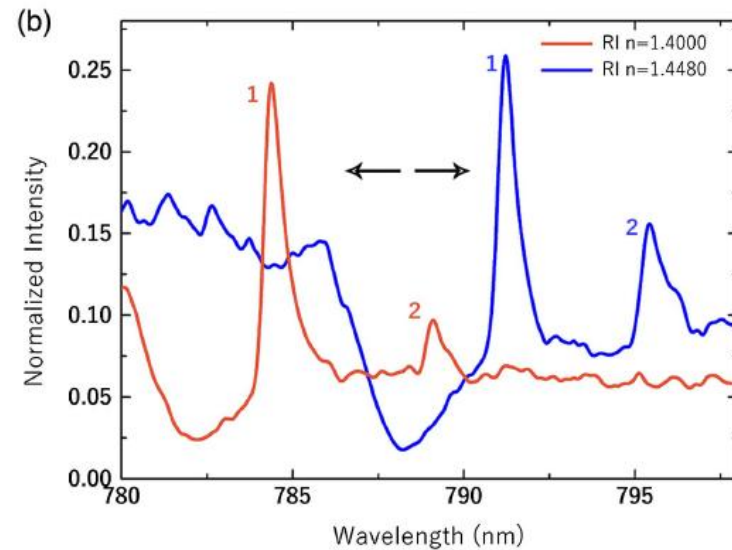
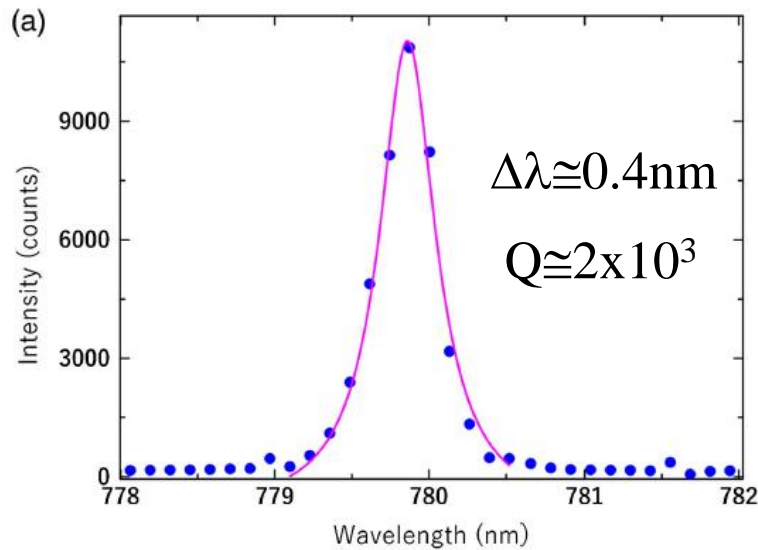
- 1) $\lambda_{\text{res}} \sim 780$ nm
- 2) $\lambda_{\text{res}} \sim 545$ nm



Device fabrication

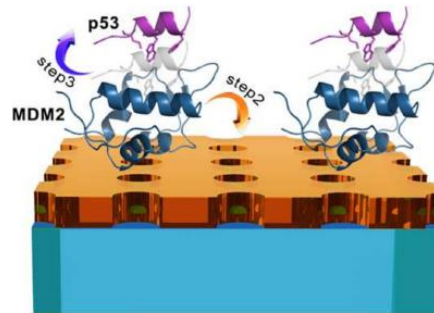


Device characterization

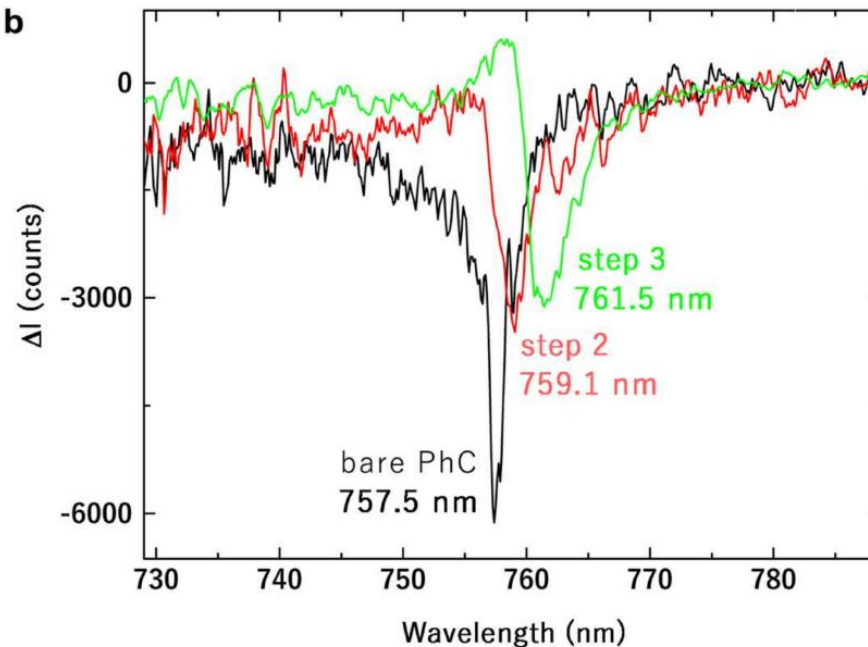


First study of MDM2-p53 protein-protein interaction

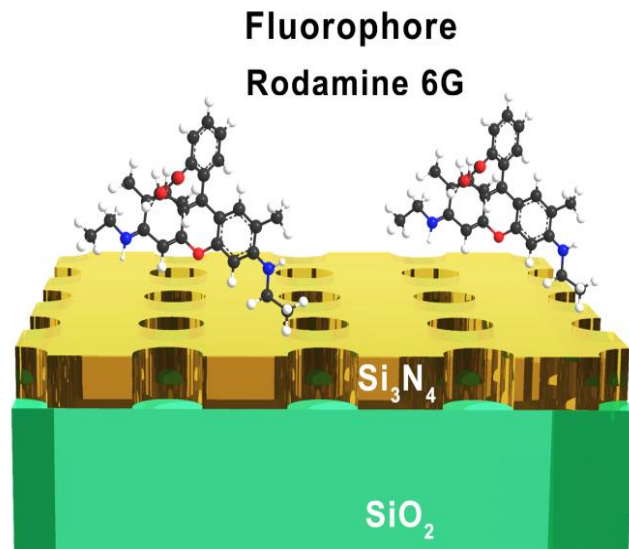
a



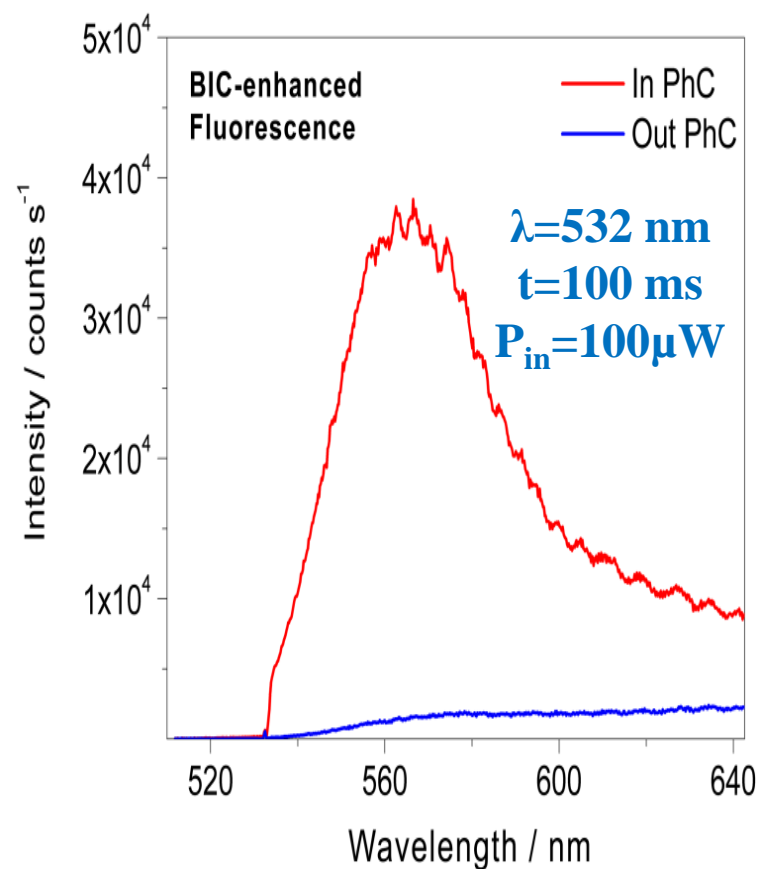
b



BIC-Enhanced Fluorescence

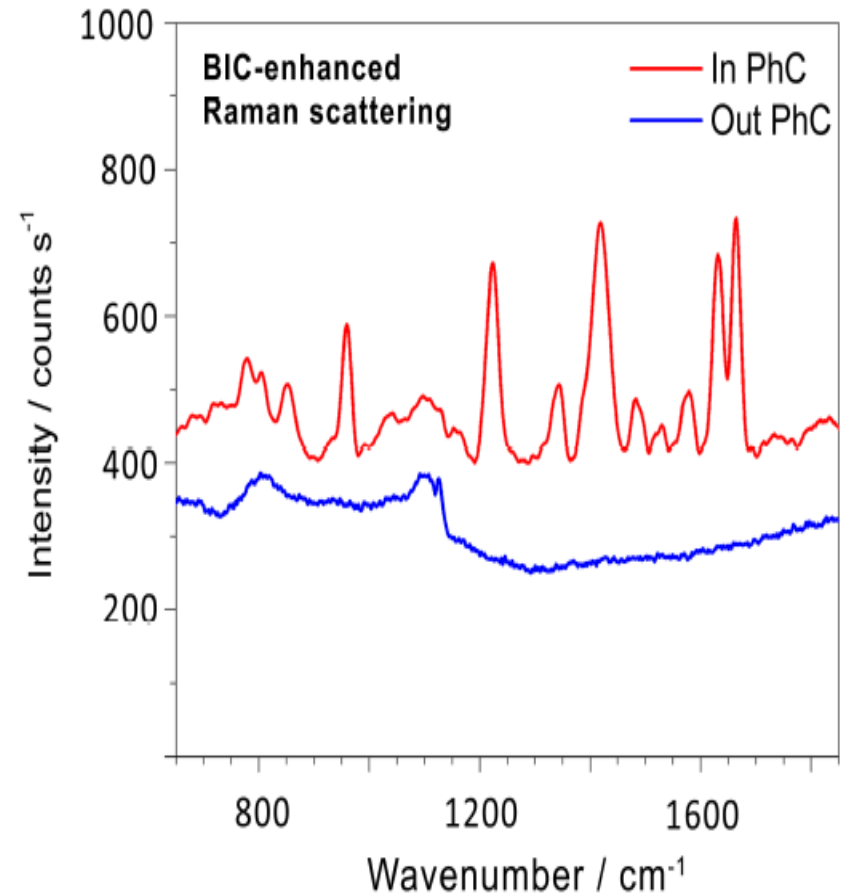
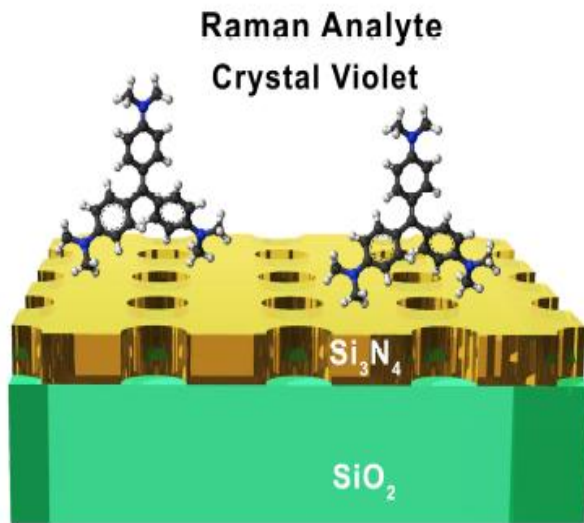


Rhodamine 6G dispersed in PMMA
C=10 μ M



SEF factor $\sim 10^3$

BIC-Enhanced Raman effect



$$F_{\text{BIC-R}} > 10^3$$

- $\lambda=532$ nm
- Crystal Violet solution in ethanol

BIC-LSPR hybrid effect

Au-NPs diameter $\cong 40$ nm

$\lambda_{\text{res}} \sim 530$ nm

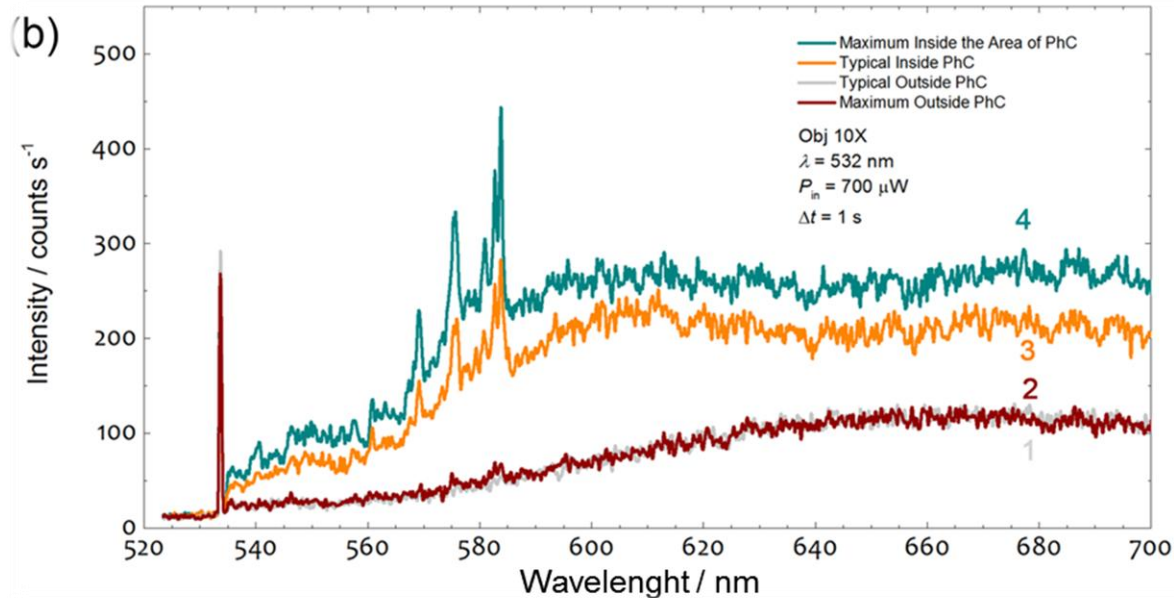
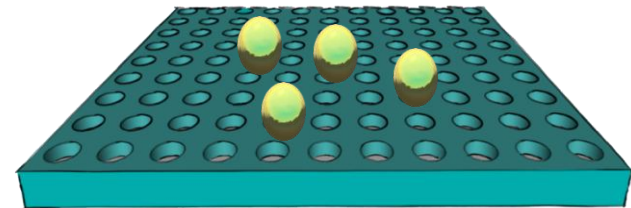
$$F_{\text{BIC-LSPR}} \approx 13$$

Randomly dispersed

Au-Nanoparticles

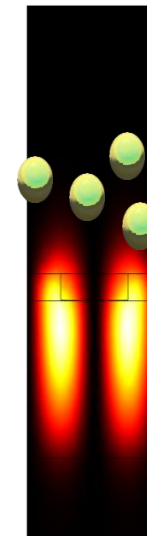


Crystal Violet molecules



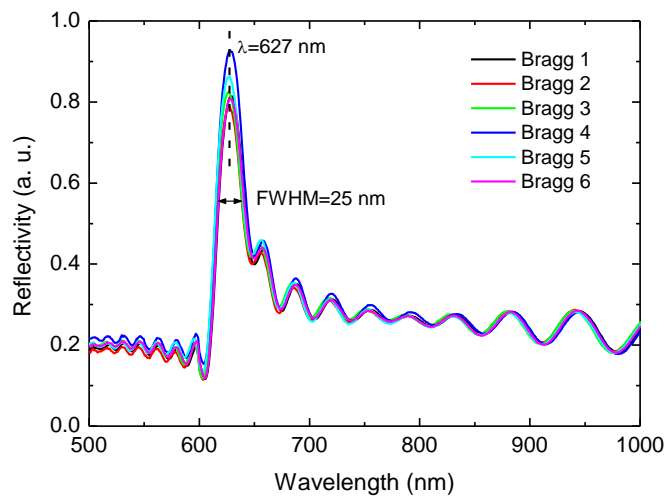
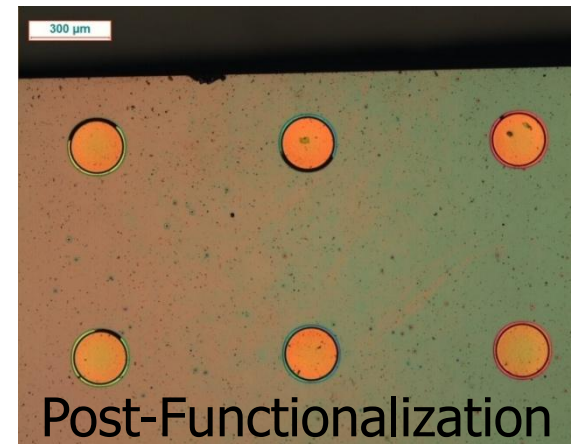
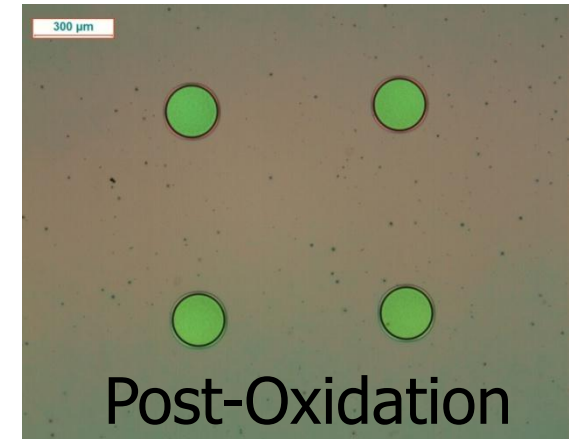
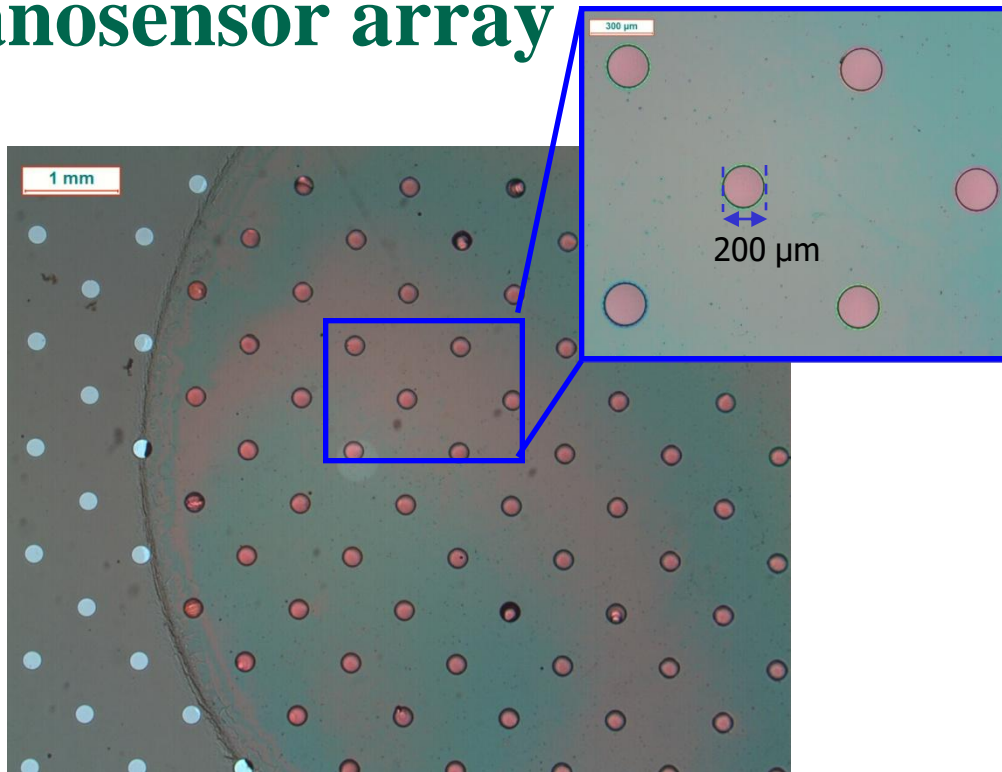
high

low

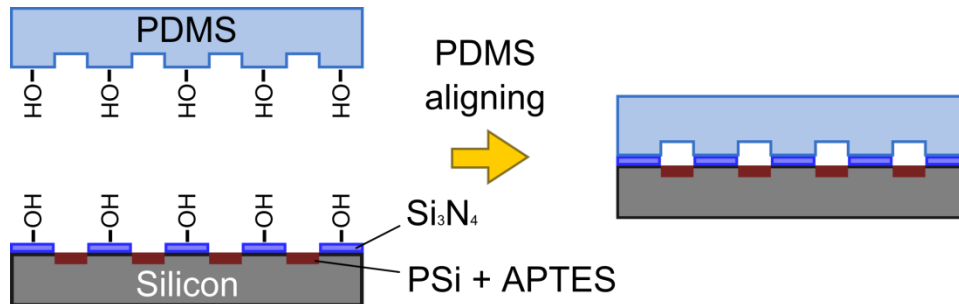


Next step:
integration with microfluidics

Nanosensor array

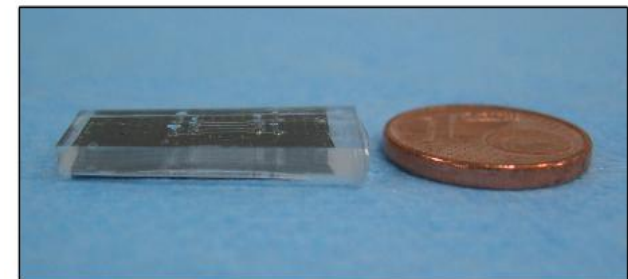
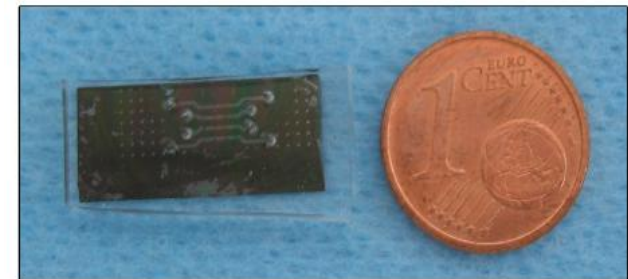
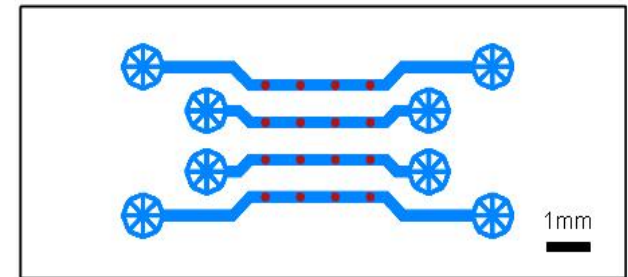


Integration with microfluidics

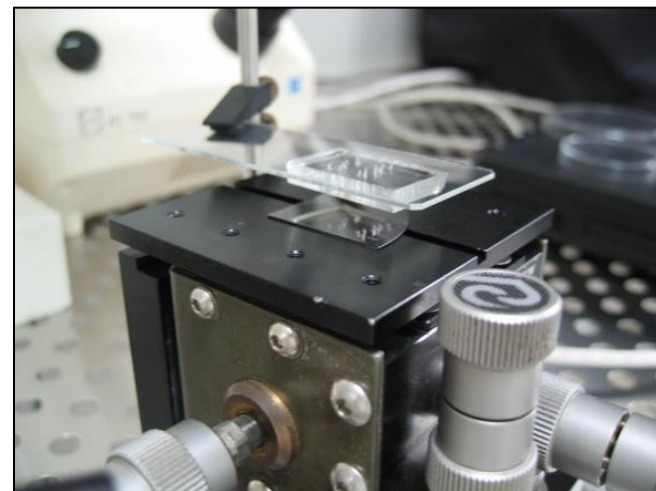


a)

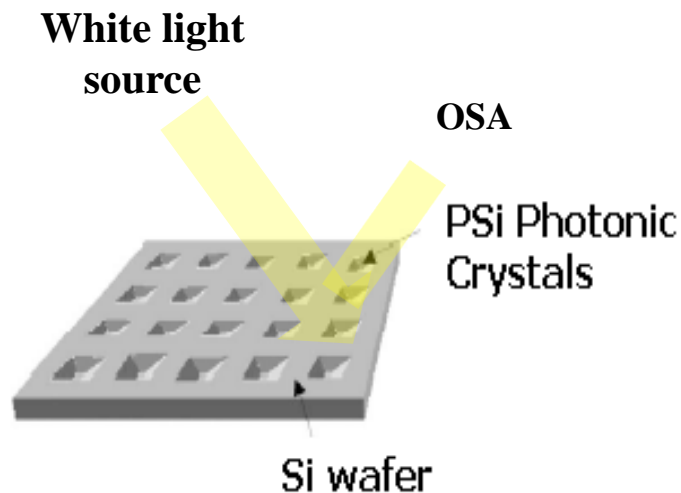
b)



Alignment
setup



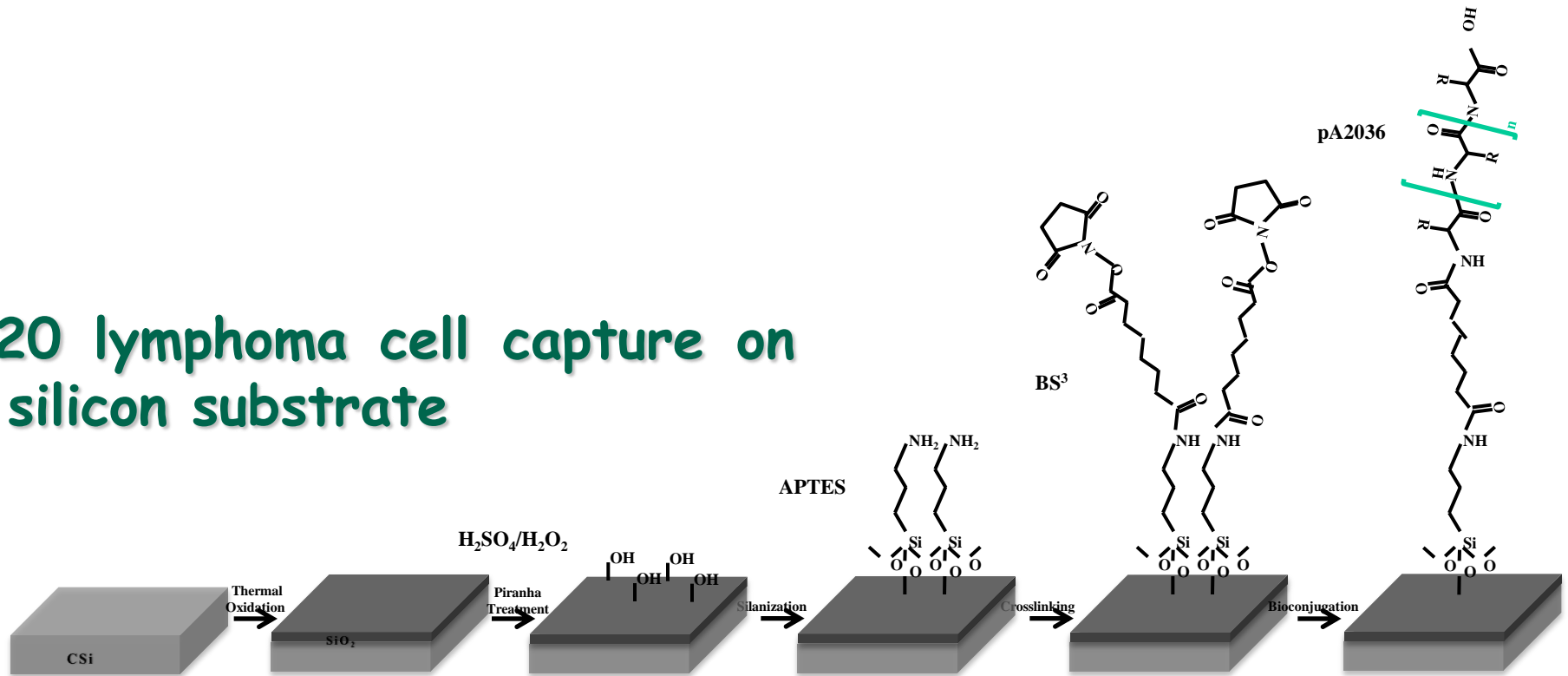
...based on a microarray of nanophotonic biosensors integrated with microfluidics



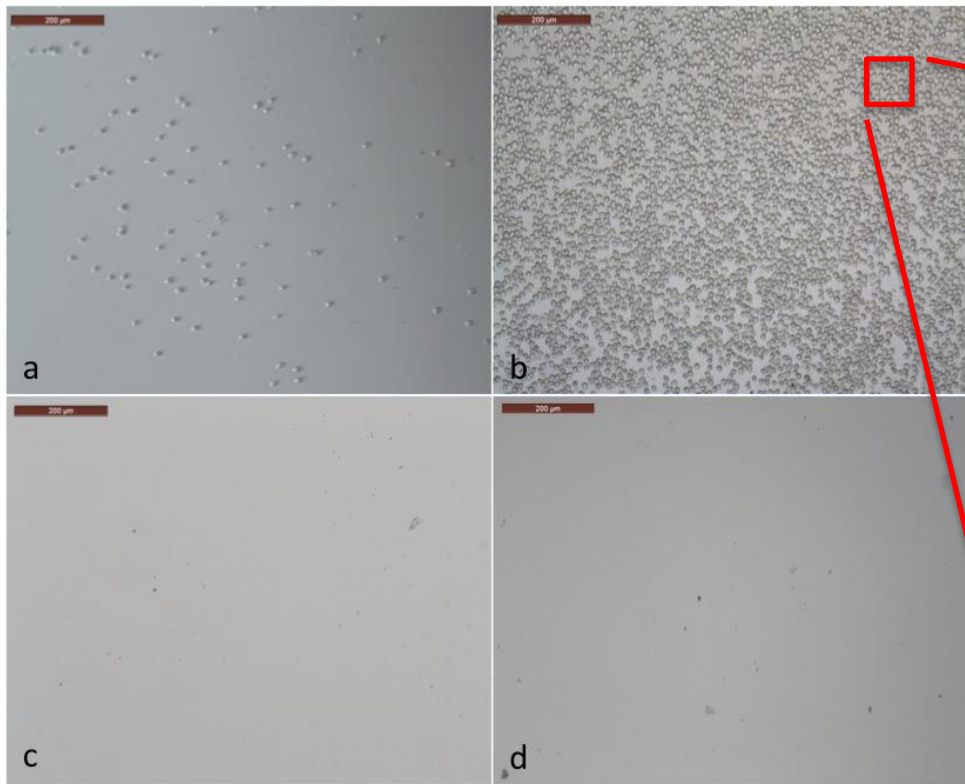
- No labeled samples
- Direct optical read-out
- Small liquid volume

Microfluidic chips for cancer cell detection:

A20 lymphoma cell capture on a silicon substrate

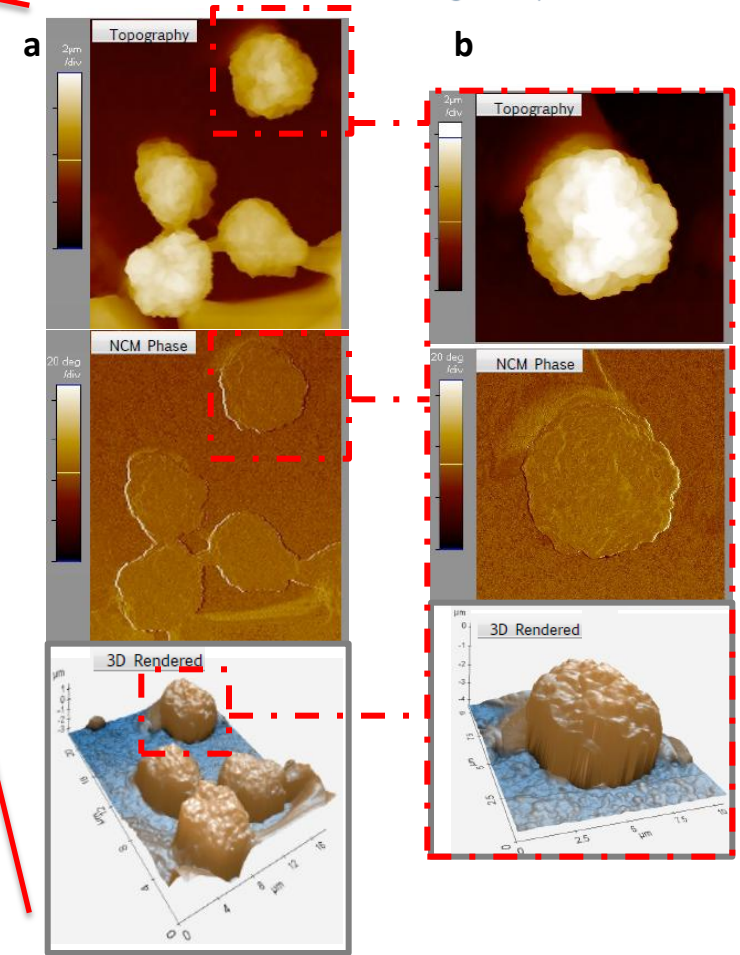


Immobilization scheme of A2036 peptide on silicon surface to detect A20 B lymphoma cells
(APTES 5% in absolute ethanol; BS³ 10mM; pA2036 150μM)



A20 cell detection on planar silicon pA2036 modified-sensor after incubation with 1×10^4 cells/mL (a) and 5×10^6 cells/mL (b).

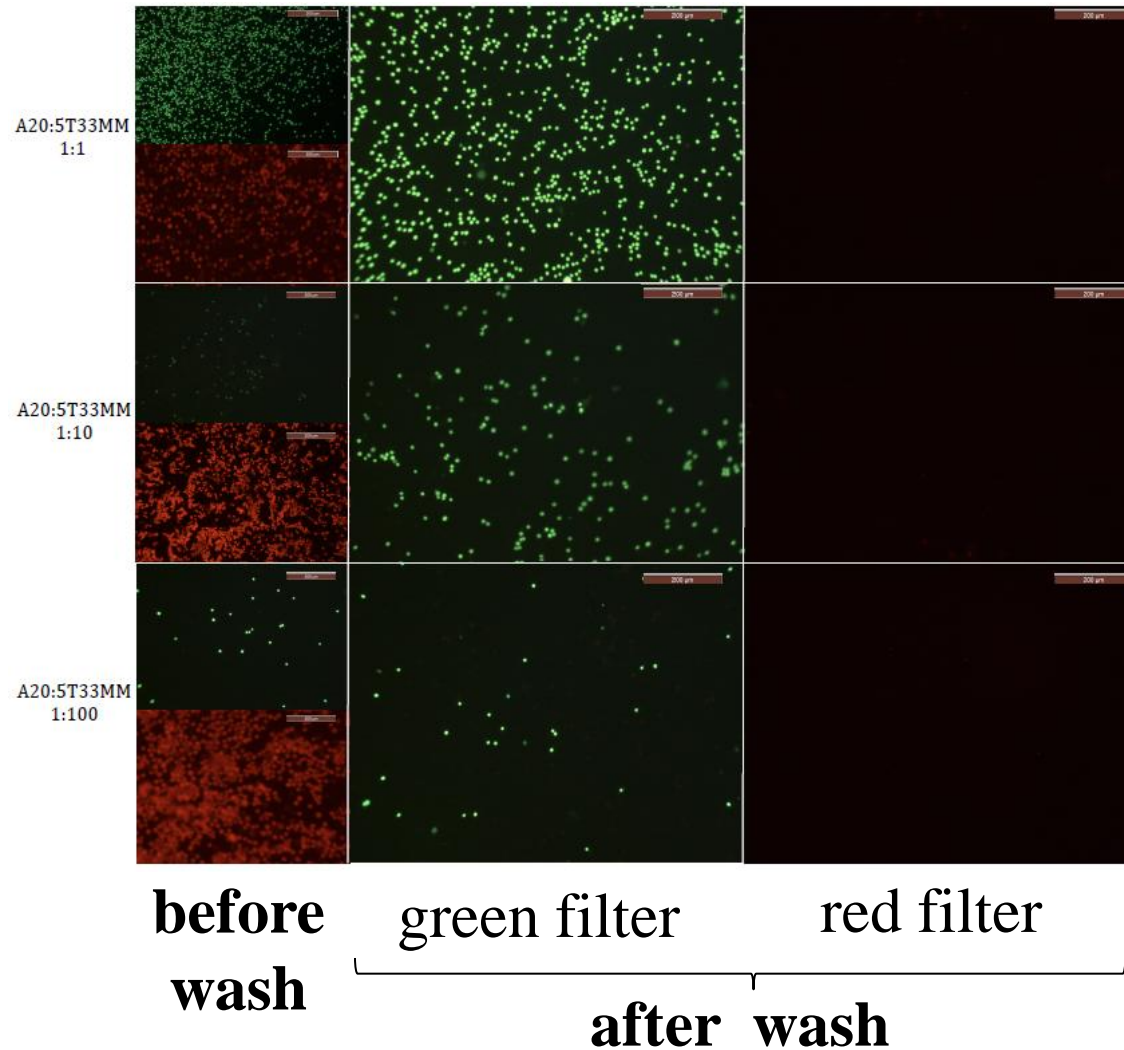
(c) Optical image of random-peptide modified-sensor incubated with A20 cells. (d) Optical image of pA2036 modified-sensor incubated with 5T33MM cells.



AFM images of live A20 cells detected on silicon surface

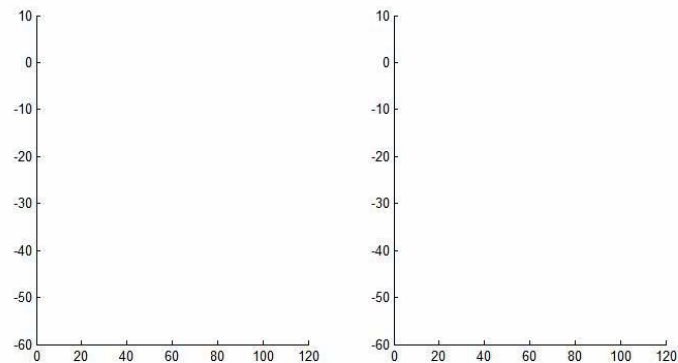
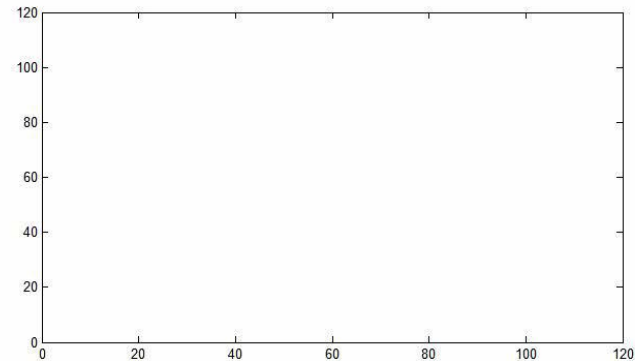
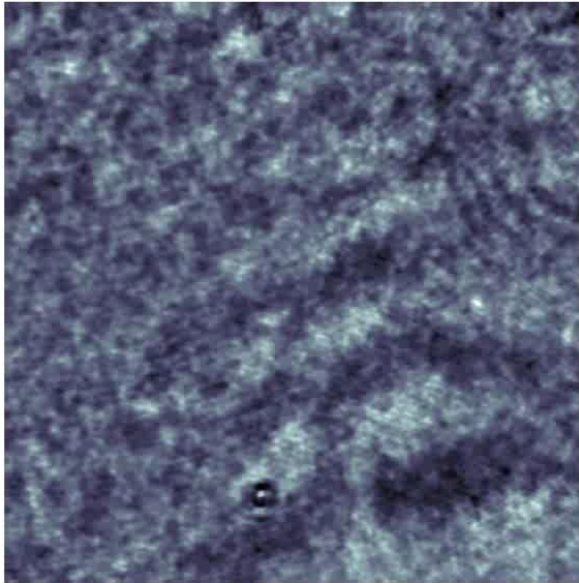
Coverage of 85% of silicon surface

A20 and 5T33MM mixed system

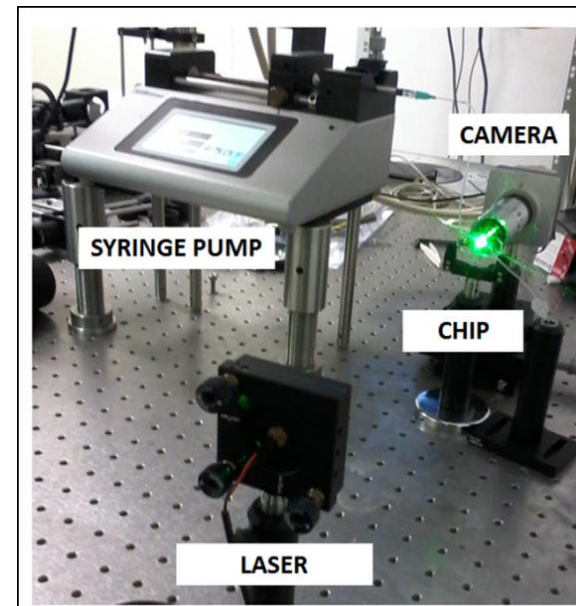
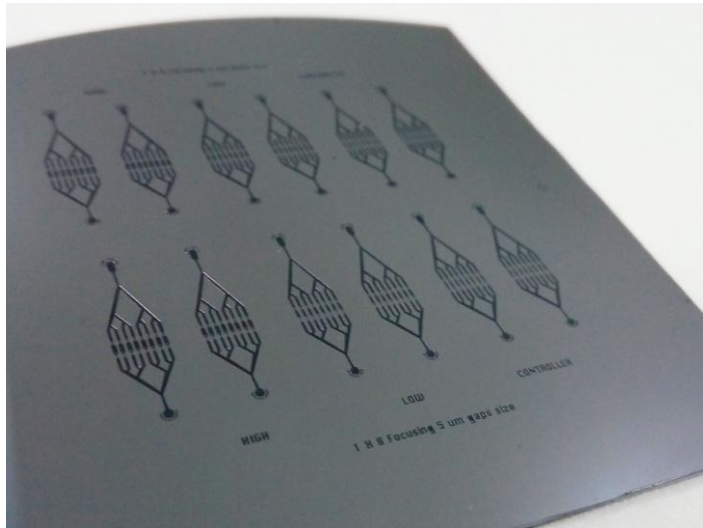
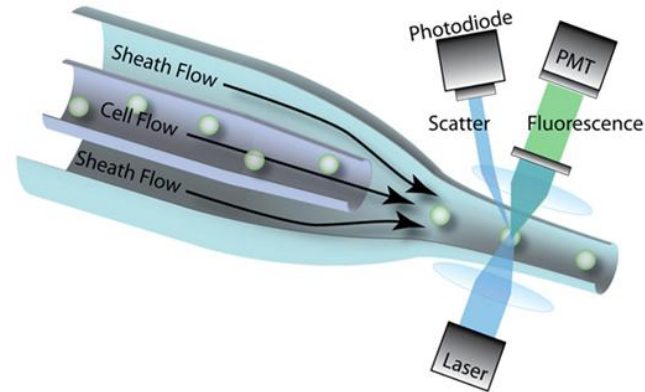


Fluorescence image of A20 cells (green) detection in system mixed with 5T33MM cells (red) on planar silicon pA2036 modified-chip after incubation at indicated ratios

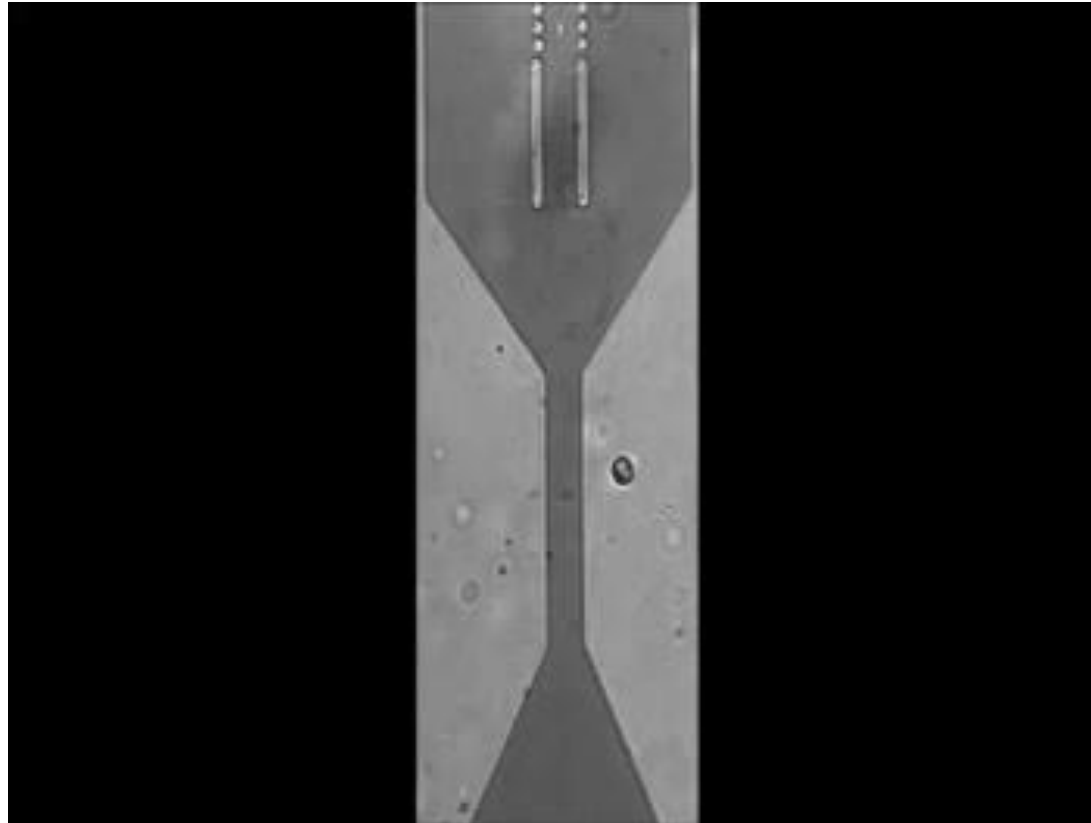
3D tracking of live cells



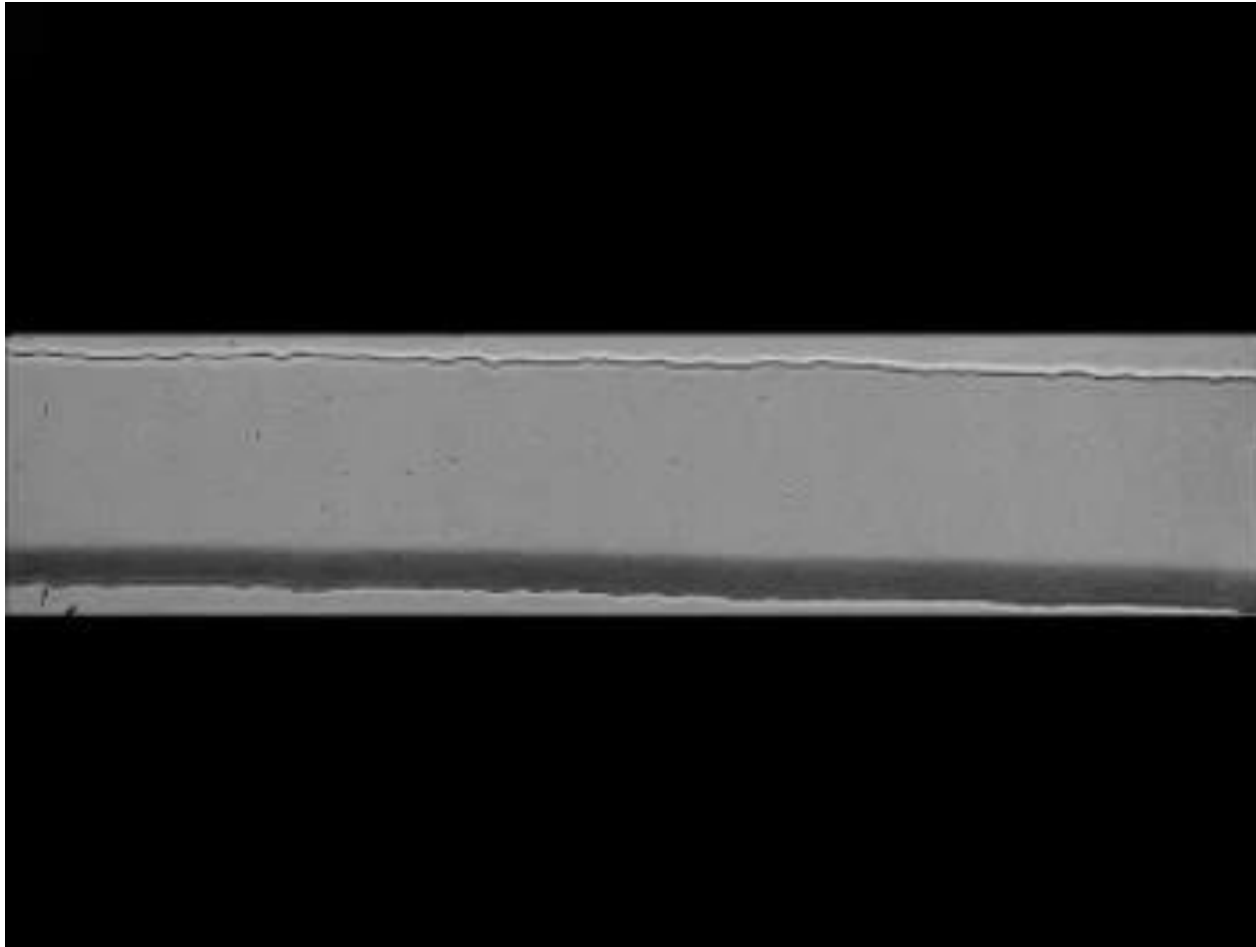
A whole flow-cytometer in a microfluidic chip



Hydrodynamic focusing of cancer cells on a silicon chip



Cell manipulation (rotation) for better on-chip imaging



The research group in Napoli



Acknowledgements



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De Luca**



Stefano Cabrini



Giuseppe Scala



Vito Mocella



Luca De Stefano



Mario Iodice



Giuseppe Coppola